

Emerging modes of collective cell migration induced by geometrical constraints

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The role of geometrical confinement on collective cell migration has been recognized but has not been elucidated yet. Here, we show that the geometrical properties of the environment regulate the formation of collective cell migration patterns through cell–cell interactions. Using microfabrication techniques to allow epithelial cell sheets to migrate into strips whose width was varied from one up to several cell diameters, we identified the modes of collective migration in response to geometrical constraints. We observed that a decrease in the width of the strips is accompanied by an overall increase in the speed of the migrating cell sheet. Moreover, large-scale vortices over tens of cell lengths appeared in the wide strips whereas a contraction–elongation type of motion is observed in the narrow strips. Velocity fields and traction force signatures within the cellular population revealed migration modes with alternative pulling and/or pushing mechanisms that depend on extrinsic constraints. Force transmission through intercellular contacts plays a key role in this process because the disruption of cell–cell junctions abolishes directed collective migration and passive cell–cell adhesions tend to move the cells uniformly together independent of the geometry. Altogether, these findings not only demonstrate the existence of patterns of collective cell migration depending on external constraints but also provide a mechanical explanation for how large-scale interactions through cell–cell junctions can feed back to regulate the organization of migrating tissues.

cell traction forces | collective dynamics | madin darby canine kidney epithelial cells | particle image velocimetry

Collective behavior is a fundamental phenomenon exhibited by a wide variety of systems such as flows in granular matter (1), collective movements of animals (2), self-organization of bacteria (3), and morphogenesis of biological tissues (4). Although collective behaviors have been observed across diverse physical and biological systems, it is increasingly clear that there are broad unifying and common parameters that govern the emergence of this phenomenon such as the density of the constituent particles, the boundary conditions within which the movements occur, and the nature of coupling between the individual particles. In this context, collective behavior in migrating cells is of particular interest as a highly out-of-equilibrium process where cells passively interact with each other and exert active forces in response to their mechanical environment (4). Such collective behavior drives many biological processes such as embryonic development (5), tissue morphogenesis (6), wound healing (7), and tumor metastasis (8, 9). Although single cell dynamics has been extensively studied (10–12), the movement of multicellular structures could not be simply explained by cell autonomous behaviors (13–16). Instead, intercellular interactions and large-scale propagation of mechanical signals (over several cell sizes) are necessary to understand the emergence of mesoscopic behaviors regulating tissue formation and cohesion (6, 17, 18).

Depending on the physiological or pathological conditions under consideration, cells can migrate as large epithelial sheets

during wound closure (7), as chains of tumor cells invading the surrounding matrix from the main tumor mass (8), or tubes of neural cells migrating along the lateral line of the zebrafish (19). Whereas studies on single cells suggest that migratory mechanisms are strongly affected by the mechanical constraints of the environment (20), the impact of such constraints on collective migration remains unclear (14, 18). However, both in vivo and in vitro collective migration behaviors occur under a broad range of external constraints that induces diverse morphological behaviors including the appearance of highly motile mesenchymal leader cells (18, 19), the organization of small cohorts of follower cells locally guided by leader cells (21), cryptic lamellipodia formation by cells several rows behind the leading front (7), and the observation of large-scale movements within cell monolayers (17, 22). Moreover, much conflicting evidence has emerged regarding the mechanical regulation of collective cell movements: in vitro traction force mapping shows that an expanding epithelial cell sheet is under a global tensile state (13), whereas recent studies on three-dimensional cell migration in tracks (23) as well as in vivo studies (24) suggest that pushing forces driven by cell-derived compression and cell proliferation could explain further cell expansion and formation of multicellular assemblies. These studies lead to important questions such as the role of the leading front in the guidance of cells behind (18, 25, 26), the influence of internal dynamics on the emergence of collective motions (16, 17), and consequently the physical mechanisms that drive collective migration under various constraints. These intriguing questions are currently debated. Understanding how external constraints influence collective cell behavior might explain some of the observed discrepancies in a large variety of biological processes.

Here, we have developed an original in vitro assay based on microfabrication techniques to determine how collective cell migration responds to well-defined geometric constraints. We show that such constraints can trigger different modes of epithelial cell migration by altering intercellular coordination within the monolayer. Mapping of the velocity field and force distribution reveals that large-scale interactions over distances spanning many cell bodies can be tuned by changing the external confinement as well as the internal dynamics of cell–cell junctions. These experimental findings supported by numerical simulations demonstrate that

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the integrated information within epithelial cell sheets, which leads to collective dynamics, is governed by interplay between external physical cues and cell–cell interactions. This study provides a framework from which the impact of external constraints on collective cell migration can be taken into account for both *in vitro* and *in vivo* studies.

Results and Discussion

Migration-Based Assay of Epithelial Cell Sheets Under Geometrical Constraints. We used a combination of various experimental techniques including microcontact printing (27), particle image velocimetry (PIV) (22), and microforce sensor arrays (28) to study the migration of an epithelial cell sheet under geometrical confinement. We designed a fibronectin pattern surrounded by nonadhesive areas (27) that includes a large rectangular reservoir connected to strips of different widths ranging from ≈ 20 to $400\ \mu\text{m}$ (*Materials and Methods* and Fig. 1A). A confluent monolayer was grown inside the reservoir adjacent to a slab of polydimethylsiloxane (PDMS). By doing so (29), we not only ensured that the monolayer was not damaged but we also allowed the cell sheet to migrate upon removal of the slab into the different strips. Providing a free virgin surface by removing the block of PDMS was sufficient to trigger the migration of Madin-Darby canine kidney (MDCK) epithelial cell sheet from the reservoir into the fibronectin strips. Using this assay, collective cell migration was strictly confined into the fibronectin patterns (Fig. 1B, *Movie S1*). After allowing the cell sheet to migrate for at least 4 h, we analyzed simultaneously cell movements within the different channels.

We first studied how the geometrical constraints influence the overall migration velocity of cell sheets. First, we computed the displacement of the leading edge of the monolayer (averaged

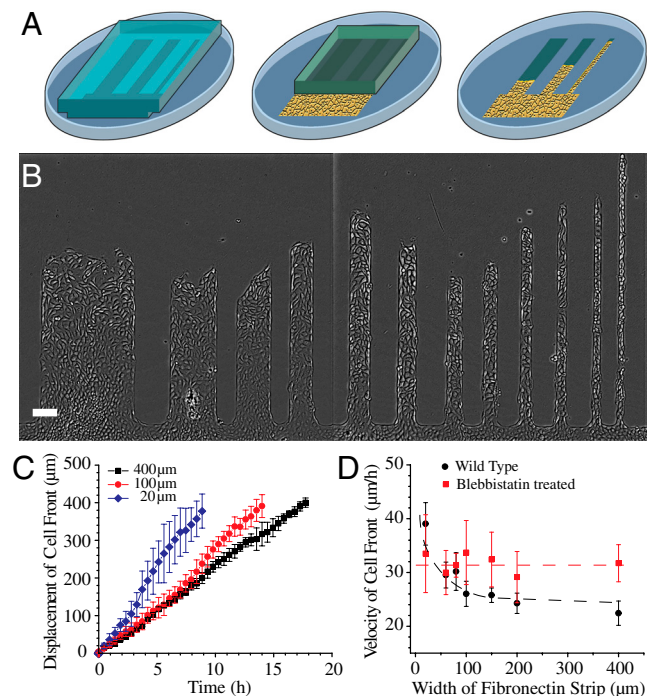


Fig. 1. Migration of MDCK cell sheet on fibronectin strips of different widths. (A) Schematic of the fibronectin stamped pattern with a block of PDMS (gray). Cells reach confluence in the reservoir (shown as a yellow area) and migrate into the strips when the PDMS block is lifted (as illustrated by the last step). (B) MDCK cell sheets migrating on fibronectin strips of different widths. (C) Average displacement of cell front over time in 400, 100, and 20- μm wide strips. (D) Velocity of cell front on strips of different widths for untreated (black) and blebbistatin-treated (red) MDCK cells. Dashed lines are a smooth fit to guide the eye. (Scale bar, 100 μm).

over several points on the leading cell front between successive images) over the whole observation period and then the average velocity as a function of the width. We observed a linear progression of the leading front independently of the width of the strip (Fig. 1C, Fig. S1A). However, we observed that the average velocity of the cell front varied with the width of the strips increasing from $22.4 \pm 2.2\ \mu\text{m}/\text{h}$ for the wider ones (400 μm) to $39 \pm 3.9\ \mu\text{m}/\text{h}$ for the narrow ones (20 μm) (Fig. 1D). Moreover, even if a linear progression of the cell front was observed for all the channels, larger fluctuations were obtained in the narrow strips (20 μm) than in the wider ones (from 100 to 400 μm) (as shown by the standard deviations of the displacement as a function of the width, Fig. 1C). In fact, a closer look into the cell sheet migration using our assay shed light on the emergence of different modes of collective cell migration. Cells in the narrow strips (20 μm) showed a contraction-relaxation or caterpillar-like mechanism to move forward (*Movie S2*), whereas those in the wide strips (400 μm) exhibited a continuous progression. We then sought to determine whether geometrical constraints could alter the shape and density of cells within the cell sheet because both these parameters could affect the migration characteristics of cell populations (30, 31). Accordingly, elongation and orientation index of cells was calculated, distribution of actin stress fibers was visualized, and cell density as a function of the distance away from the leading front was computed. Cells were found to be much more elongated and oriented along the length of the strip in the narrow (20 μm) strips whereas they had no preferred orientation in the wide and intermediate width (400 and 100 μm) strips. Furthermore, some cells at the leading front on the wider strips occasionally developed large lamellipodia and assumed a mesenchymal phenotype reminiscent of leader cells described in previous studies (21). The elongation factor was found to be 1.82 ± 0.05 on the 400 μm and 1.91 ± 0.03 on 100 μm wide strips and increased to 2.52 ± 0.16 in the 20 μm wide strips (Fig. 2A). Actin stress fibers were also found to be randomly distributed in the 400 and 100 μm wide strips but directed along the long axis of the strip in the 20 μm wide strips (Fig. 2B). Furthermore, on the 400 and 100 μm wide strips, cell density increased from approximately 1 cell/1,000 μm^2 at the leading front to approximately 4 cells/1,000 μm^2 about 600 μm away from the

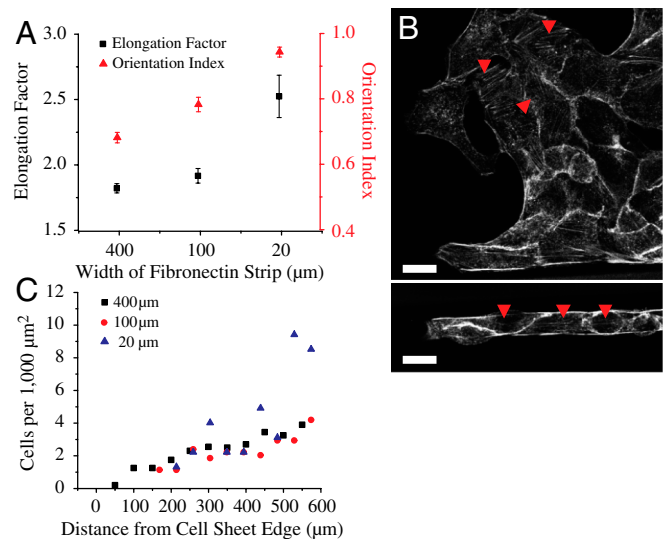


Fig. 2. Width of the fibronectin strip affects the morphology and cell density in the migrating epithelium. (A) Elongation factor and orientation index in strips of different widths. (B) Actin staining showing random stress fiber distribution in the 400- μm wide (arrow heads, *Upper*) and aligned stress fibers in the 20- μm wide strips (arrow heads, *Lower*). (C) Cell density at different distances from the leading front on strips of different widths. (Scale bars, 20 μm).

contrast images (Movie S2). A closer analysis of the migration revealed that the contraction-relaxation cycle in the narrow strips spans $\approx 100 \mu\text{m}$ ($\approx 3\text{--}6$ cells, Fig. S1B). Such alternating phases of acceleration and stalling appear to be reminiscent of the extension of finger-like shapes in migrating epithelia as previously described (26). However, this observation suggests that although the leading front is important in driving migration of cells into the strips, cell-cell interactions far away from the leading edge also actively contribute to the net progression of the cell monolayer. Interestingly, the magnitudes as well as fluctuations in velocities were higher on the edges of the wider strips rather than in the middle of the strip (Fig. S1C). Because cells in this region are confined only on one side, they experience an intermediate behavior between cells in the middle of the wide strip and those in the narrow strips. To further delineate the role of large-scale coordinated movements and correlation length of such movements in regulating the migration modes, we analyzed the direction of the velocity vectors. Large and transient vortices of $\approx 100 \mu\text{m}$ in diameter (approximately 10 cells) were observed in the $400 \mu\text{m}$ wide strips but not in strips of widths $\leq 100 \mu\text{m}$ (Fig. 3A, Middle and Right and Movies S4 and S5) in agreement with previous studies based on traditional wound healing assays (30). Consequently, we measured the spatial velocity correlation along the length (ξ_v) and width of the channel (ξ_u), which quantified the distances over which the movements were collectively driven within the monolayer. Previous studies on epithelial cells have shown that large unconfined migrating monolayers led to similar finite values of the correlation lengths within a range comprised between 120 to 200 μm (Fig. 3F) (30, 32, 33). Here, the correlation length ξ_u scales with the width of the strips for strips whose width was $\leq 100 \mu\text{m}$. However, in strips $>100 \mu\text{m}$ wide, ξ_u saturates quickly reaching a value of approximately 100 μm , reflecting mostly the internal dynamics of the monolayer (Fig. 3F). Interestingly, a similar relationship has been previously described for other physical systems such as sedimenting colloids (34). The velocity fluctuations in colloidal sedimentation varied with the width of the confinement only for dimensions smaller than the characteristic swirl size. By plotting the average velocity fluctuations (perpendicular to the length of the strip) as a function of the width of the fibronectin strips (Fig. S1E), we found that these fluctuations scaled with the width of the strip in a fashion similar to that observed for the correlation length. In the parallel direction of the strip, the correlation length, ξ_v , shows a nearly constant value (approximately 100 μm) as a function of the width (Fig. 3F). Consequently, it appears that geometrical constraints are sufficient to modulate the dynamics of cell-cell interactions and induce large-scale alignment of cells. To confirm that the geometrical constraints govern a transition in the polarized migration of the multicellular assemblies, we computed the order parameter (SI Materials and Methods and Fig. 3G) of the velocity vectors. The quantification of this parameter exhibits a significant decrease from 0.92 to 0.79 when increasing the width of the channel from 20 to 400 μm , respectively. These observations are well-supported by recent numerical results showing that the length scale of geometrical constraints could have a strong influence on the emerging directionality in cell populations, irrespective of the dynamics of a leading edge and of potential proliferation effects (35). Considering a population of $N \times N$ motile cells confined in a biperiodic domain, the model exhibits a transition from sheet migration (full alignment) to swirls (no overall alignment) as the size N of the system is increased from a few cells to tens of cells. Consistently with the experiment, the alignment transition is found to occur when N is of the order of the correlation length of the unconstrained case (SI Materials and Methods and Fig. S1D). This similarity suggests that such a transition is a physical process driven by the internal dynamics of the cell sheet although the overall directionality and caterpillar-like dynamics are still governed by the leading front as described by other models (26).

In particular, the order parameter in the experimental system tends to a finite value at large channel widths, consistent with wound healing assays, rather than zero as expected in the simulation. Together, these observations establish that physical constraints affect cell-cell rearrangements and thus the active forces exerted through cell-cell junctions.

Role of Cell-Cell Junctions in Epithelial Cell Migration. Because cell-cell interactions appeared to play a key role in the observed modes of migration, we examined the role of intercellular adhesion proteins. Cell-cell junction proteins such as E-cadherins and their linkage to actin cytoskeleton through various cytoplasmic adaptor molecules (e.g., α -catenin) are crucial to maintain the cohesiveness and physical integrity of epithelial cell sheets (36). Immunostaining for E-cadherin revealed that intercellular contacts were intact in strips of all widths (SI Materials and Methods and Fig. S2). To assess further the importance of cell-cell adhesion for coordinated collective migration, we analyzed the migration of MDCK cells in which α -catenin has been stably knocked down and hence cannot form stable intercellular contacts (36). These cells migrated in a highly uncoordinated and random fashion leading to significantly lower migration velocity (approximately 13 $\mu\text{m}/\text{h}$ across fibronectin strips of all widths) of the overall cell front compared to normal MDCK cells (Movie S6). A similar migratory behavior was also observed in low calcium medium (Movie S7). Together, these results show that intercellular transmission of mechanical signals across many cells is crucial to observe long-range interactions within the monolayer as well as directed and cohesive motions.

Substrate Traction Forces Reveal Different Modes of Migration. We further hypothesized that the emergence of various modes of migration depending on geometrical confinement could appear as distinct signatures in the magnitude, orientation, spatial, and temporal distribution of substrate traction forces exerted by the cell sheet. To explore this hypothesis, cell sheets were allowed to migrate on strips of flexible micropillars with similar dimensions as the ones previously described (28). As shown by SEM pictures (Fig. S3A) and immunostaining experiments (Fig. 4A and Fig. S3B), the cells were nicely confined on the strips, adhered on the top of the micropillars, and were able to deform the pillars (Fig. 4B). We then used live-cell video microscopy to obtain quantitative values of the traction forces exerted by the epithelial cells (see Materials and Methods). The average traction force, $\langle F \rangle$, registered in the $400 \mu\text{m}$ wide strips were higher at the leading front ($2.27 \pm 0.19 \text{ nN}$), decayed rapidly by 50% to $1.14 \pm 0.12 \text{ nN}$ at approximately 100 μm away from the front (Fig. 4B) and were randomly oriented in all directions (Movie S8). We observed larger traction forces at the leading front on the 20 μm wide strips ($2.74 \pm 0.26 \text{ nN}$). However, whereas $\langle F \rangle$ exhibited a monotonic decay as a function of the distance from the edge in the $400 \mu\text{m}$ wide strips, $\langle F \rangle$ showed spikes of forces (approximately 2 to 2.5 nN) much further away from the leading front (Fig. 4B), which were predominantly directed along the length of the strip (Movie S9). In an attempt to correlate the traction forces to the differences in migratory patterns observed with PIV, we analyzed the stress ($\langle \sigma_{xx} \rangle$) within the cell sheet along the length of the strip in the 400 and 20- μm wide strips (Fig. S3C). As previously described by Trepate et al. (13), the stress, $\langle \sigma_{xx}(D) \rangle$, at a given distance D from the leading edge was obtained by summing the traction forces exerted by cells in the x -direction from the leading edge up to the distance D according to mechanical equilibrium. Our results showed that $\langle \sigma_{xx} \rangle$ initially increased sharply for the cell sheet migrating on 400- μm wide strips (Fig. S3D). Such a profile of stress distribution indicated that cells several rows behind the leading front also contributed to the migration of the cell sheet in agreement with previous studies (13, 28). Interestingly, $\langle \sigma_{xx} \rangle$ was found to be lower on the 20- μm wide strips

the order parameter (Fig. 3G) and the restricted migration along the length of the channels. In the same line, both theoretical (26) and experimental (38) studies suggest that geometrical confinements could reduce the instabilities of the cell front described as finger-like structures and thus promote the higher observed velocities. However, the large velocity fields and traction forces observed far away from the leading cell front in the narrow channels suggest that the local coordination also originates from the interactions with the boundaries of the strips rather than with the leading edge only. The correlation length displays a dependence on the channel width but only for those which are smaller than the correlation length attributed to the intrinsic dynamics of the epithelial cells (approximately 100 μm) similar to passive physical systems (34). However in our case, the dynamics of cell sheets is strongly driven by active processes which increase the complexity of the observed interactions. The dynamic behavior observed in our experiments could be determined by a multitude of physical and biological factors. Here we quantitatively demonstrated that the geometrical constraints as well as cell–cell interactions played a critical role in the collective migration of cells but other parameters such as cell density as well as the nature of the substrate can affect the long-range interactions in migrating MDCK cells (30, 32).

The systems behavior, as the width of the strip is varied, is reminiscent of phase transition observed in various systems from a relatively disordered regime to a more orderly behavior in response to changes in local density of the constituent particles (39–41). The numerical results have in particular confirmed that such a physical approach could account for the evolution of the order parameter as the width is varied. Altogether, our results show that geometrical constraints lead to the emergence of a

more directed and ordered migration when the population is confined below its natural correlation length, which in turn is controlled by cell–cell interactions. Such modes of migration could indeed be altered by changes in the dynamics of mechanical interactions mediated by intercellular adhesion because isolated MDCK cells, MDCK cells treated with blebbistatin, as well as α -catenin knockdown cells exhibit highly altered collective dynamics. Because tissue migration comes in many shapes and sizes (25) and our results shed a unique perspective on how collective cell migration should be reinterpreted depending on its guidance by extrinsic cues.

Materials and Methods

The fibronectin pattern studied here consists of a large rectangle (reservoir) joined to strips of varying widths (approximately 400 to 20 μm , Fig. 1). Microcontact printing was performed using PDMS stamps inked with a mixture of fibronectin and Cy3-conjugated fibronectin (27). A block of PDMS was placed on the pattern to cover the strips leaving the reservoir open for seeding cells. Particle image velocimetry (PIV) and micropillar arrays were used for analyzing velocity fields and traction forces, respectively. (See *SI Materials and Methods* for a detailed description).

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Supporting Information

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SI Text

SI Materials and Methods. Stamp preparation, cell seeding, and microscopy. Polydimethylsiloxane (PDMS) stamps for microcontact printing were prepared as described before (1). Molds of the pattern were first prepared using standard lithography methods. PDMS (Sylgard 184; Dow Corning) was prepared by mixing the base and curing agent in a ratio of 1:10 (wt/wt) and degassed. It was poured over the mold, degassed, and cured at 80 °C for 1 h. Stamps were peeled off the molds and plasma cleaned to make their surface hydrophilic. A mixture of Cy3 conjugated fibronectin and normal fibronectin (50 µg/mL; Sigma) was added immediately over the stamps to cover the whole surface. The mixture was allowed to be adsorbed for 45 min after which the excess fibronectin was removed with a pipette. The stamps were left in the laminar hood for approximately 10 min to dry. They were then gently pressed against the bottom of a non-culture-treated petri dish (Greiner) for about 1 min. The stamps were then carefully lifted up and the petri dishes were thoroughly rinsed with PBS. The patterns were visualized under a fluorescence microscope (Nikon). Petri dishes in which the fibronectin patterns were transferred properly were treated with a solution of 0.2% Pluronic F127 (Sigma) for 1 h to prevent cells from attaching and growing on the unstamped areas. After the incubation, the dishes were thoroughly rinsed several times with PBS to remove excess Pluronic F127.

Madin-Darby canine kidney (MDCK) cells were maintained in DMEM (Sigma) supplemented with 10% FBS (Hyclone) and 1% penicillin and streptomycin. Cells were seeded close to the edge of the PDMS block placed on the pattern and incubated overnight. The medium was removed the next day to wash off the unattached cells following which the PDMS block was lifted off. The petri dish was rinsed again with PBS to remove floating cells. Finally, culture medium was added and the petri dish was mounted on a microscope equipped with temperature, humidity, and CO₂ control (Olympus IX81) for live imaging. For some of the experiments, image acquisition was performed on Biostation (Nikon). Phase contrast images were acquired every 4 min using a 10× objective. Acquisitions were typically obtained over a period varying from 12 to 24 h. For inhibiting myosin II, blebbistatin (stock 100 mM in DMSO; Tocris) was added at a final concentration of 50 µM after removing the PDMS block. Because the Biostation uses red light for illuminating the sample, there was no observable phototoxicity of blebbistatin.

Preparation of micropillars for traction force microscopy. Molds of silicon wafers containing the patterns (prepared using reactive ion etching) were first silanized. PDMS was poured onto the molds and allowed to cure at 120 °C for 15 min. The elastic modulus of PDMS cured under these conditions was found to be approximately 290 kPa, which translated into a spring constant of 10 nN/µm for the micropillars. The PDMS micropillars were gently peeled off in absolute alcohol and dried using a critical point dryer (Toussimis, Autosamdri-815) to prevent their collapse. Flat blocks of PDMS were incubated with a mixture of fluorescent and normal fibronectin (50 µg/mL) for 1 h. The solution was drained off and the stamps were dried thoroughly. The pillars were exposed to ultraviolet light in a UV cleaner (Nanoscience) for 30 min and stamped using the PDMS blocks prepared above. Stamping was confirmed using fluorescence microscopy. The pillars were then incubated in a 0.2% solution of Pluronic F127 (Sigma) for 30 min and then washed thoroughly with PBS. As described in the earlier section, a PDMS

block was placed on the pillars such that it left the reservoir open for seeding cells. After cells reached confluence in the reservoir, the PDMS block was lifted to allow for cells to migrate into the channels containing arrays of micropillars. Fluorescent images of the top of the pillars were collected every 15 min for approximately 16 h on an upright microscope (Zeiss) equipped with an incubation system using a 63× water immersion objective and coupled to an electron multiplying charge coupled device camera.

Image analysis. Particle image velocimetry (PIV) was performed using MatPIV package and implemented in MATLAB (2). Background subtractions of the input images were first performed in Image J to remove noise. Single cells ($n > 10$) were tracked using the manual tracking plugin for Image J and the result was used as input to determine the size of interrogation window for PIV as well as to confirm the accuracy of PIV. The correlation coefficients and curl of the velocity fields were also calculated in MATLAB. For traction force microscopy, images were first pre-processed in Image J to enhance contrast and subtract background. Drifts in the images were removed using an image stabilizing plugin [Image stabilizer plugin for ImageJ (3)]. Micropillars were 2 µm in diameter, 4 µm in height with a center to center spacing between the pillars of 4 µm. Pillar deflections were computed from the fluorescent images using a slightly modified custom code described previously (4). The noise level in the force measurement was estimated to be approximately 0.4 nN by averaging the forces registered in regions not covered by cells.

Staining and fluorescence microscopy. Cells were grown on patterned PDMS stamps coated with fibronectin. Cells were fixed for 15 min in 4% paraformaldehyde and permeabilized for 10 min using 0.1% Triton X-100 in PBS. For visualizing actin network, the fixed and permeabilized cells were incubated with Alexa488-labeled phalloidin for 30 min. To stain for E-cadherin, cells were fixed and permeabilized in ice cold methanol for approximately 3–5 min, blocked in a solution of 3% BSA in 0.1% Triton X-100 for 1 h, incubated with mouse primary antibody against E-cadherin (1:50 in blocking solution) for 1 h and finally incubated with Alexa488-conjugated goat anti-mouse antibody. Cells were washed with PBS and then mounted using Fluorsave (Calbiochem). Images were acquired on a confocal microscope (Leica SP5).

Calculation of the elongation factor, orientation index, order parameter, correlation coefficients, velocity fluctuations, and curl of velocity fields. Elongation factor and orientation index were computed by considering individual cells ($n > 30$) as ellipses. Elongation factor is the ratio of the major and minor axis and the orientation of the cell is considered to be the cosine of the angle between the major axis of the cell and the length of the fibronectin strip. The order parameter was defined as the cosine of the angle that the velocity vector makes with the length of the fibronectin strip. The order parameter varies from +1 (for velocity vectors parallel to the strip and directed along the direction of migration of the cell sheet) to -1 (for vectors that are directed opposite to the direction of migration of the cell front) through 0 (for those vectors that are directed perpendicular to the length of the strip).

The correlation coefficients were calculated using the following formulas:

$$C_u(\vec{r}) = \left\langle \frac{\langle u^*(\vec{r}' + \vec{r}, t) \times u^*(\vec{r}', t) \rangle \vec{r}'}{[\langle u^*(\vec{r}' + \vec{r}, t)^2 \rangle \langle u^*(\vec{r}', t)^2 \rangle]^{1/2}} \right\rangle t$$

$$C_v(\vec{r}) = \left\langle \frac{\langle v^*(\vec{r}' + \vec{r}, t) \times v^*(\vec{r}', t) \rangle \vec{r}'}{[\langle v^*(\vec{r}' + \vec{r}, t)^2 \rangle \langle v^*(\vec{r}', t)^2 \rangle]^{1/2}} \right\rangle t$$

where C_u and C_v refer to the correlation coefficients in the directions perpendicular and parallel to the long axis of the fibronectin strip, respectively, u^* and v^* refer to the deviation of the velocity from the mean velocity in the directions perpendicular and parallel to the strip, \vec{r} is the vector of the coordinates, and t refers to time. The spatial velocity correlation functions were evaluated by averaging the correlation coefficient over all the directions such that C_u and C_v are now functions of $\|\vec{r}\|$ (the norm of \vec{r}). The correlation length is the distance ($\|\vec{r}\|$) where the spatial velocity correlation function become zero. Velocity fluctuations perpendicular to the strip (ΔU) were computed by subtracting the average of the perpendicular component of all the velocity vectors and normalized by the average velocity of the migrating cell front (V_{mean}). The curl of the velocity fields gives an estimate of the rotation of the vectors over time. The curl function is defined as follows:

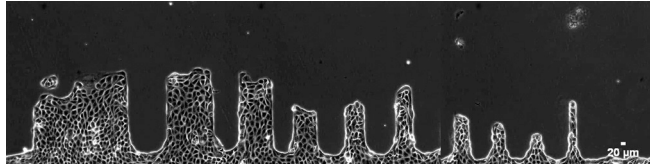
$$\nabla = \frac{\partial v}{\partial x} - \frac{\partial u}{\partial y}.$$

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5. Graner F, Glazier JA (1992) Simulation of biological cell sorting using a two-dimensional extended Potts model. *Phys Rev Lett* 69:2013–2016.
6. Szabo A, et al. (2010) Collective cell motion in endothelial monolayers. *Phys Biol* 7:046007.
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Actual computation was implemented using the in-built curl function in MATLAB.

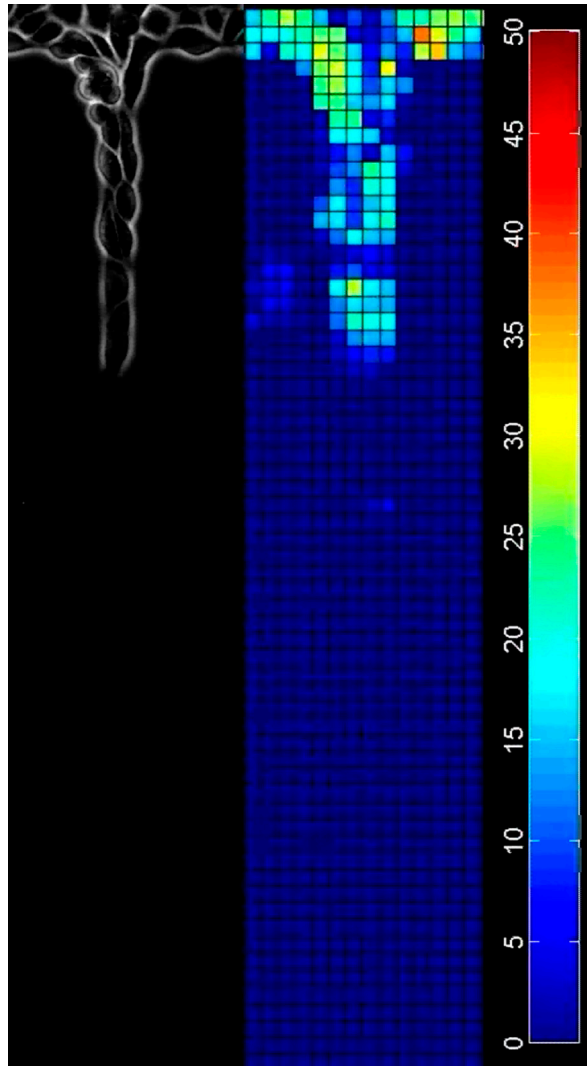
Numerical simulation The numerical model is based on self-propelled cells interacting through adhesion and excluded volume interactions. The polarity of each cell, controlling the direction of its motile force, evolves as a result of a feedback from the cell displacement, with a certain persistence time. This framework, implemented using a cellular Potts model (5), proved to quantitatively reproduce correlations patterns in dense MDCK cell populations (6). The particular code used here has been described and characterized in ref. 7. The main physical parameters of the model are the membrane energy, the cell motile force, and the persistence time of the cell polarity. These quantities account for cell stiffness, cell adhesion, and cell migration, and control the correlation length of the cell velocities in unconstrained conditions.

To test quantitatively if the simple mechanical interactions introduced in the model can explain the change in behavior between wide and narrow channels, simulations were run with parameters such that the unconstrained correlation length is comparable with the experimental value (about 10 cell diameters). The model was used to simulate dense populations of $N \times N$ cells confined in a biperiodic domain, for values of N ranging from 3 to 40 cells. The order parameter in the population was then calculated and plotted as a function of the population width N (Fig. S1D) to allow comparison with Fig. 3G.



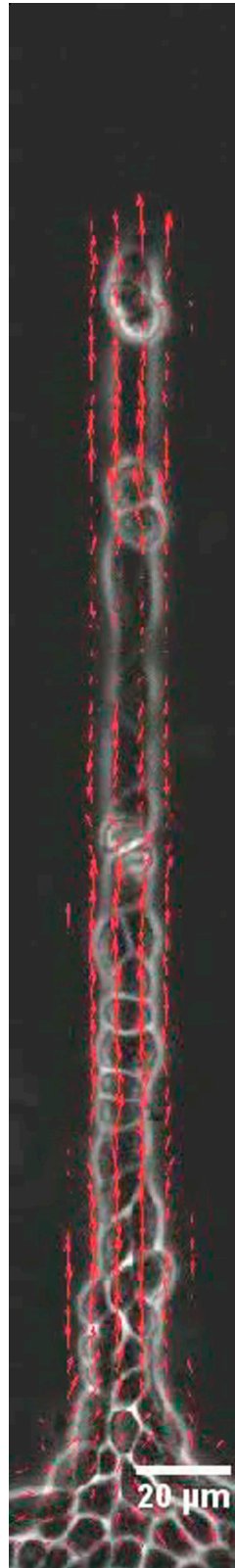
Movie S1. Migration of MDCK cells into fibronectin strips of different widths after the removal of a barrier. (Scale bar, 20 μm).

[Movie S1 \(MOV\)](#)



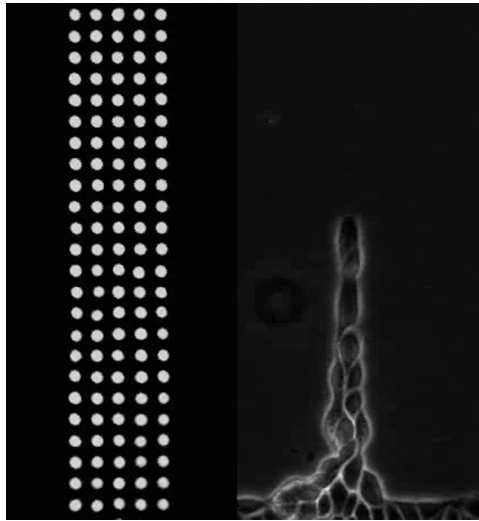
Movie S2. Caterpillar-like mode of migration in the 20- μm wide strip (*Left*) and magnitude of the velocity fields obtained using PIV (*Right*). Each frame is 20 min apart and video is played at 7 frames per second.

[Movie S2 \(MOV\)](#)



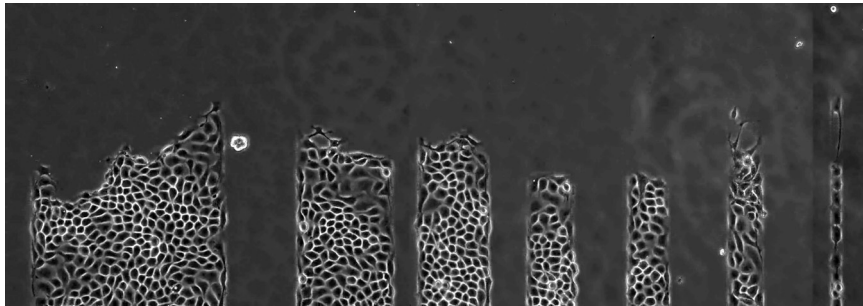
Movie S5. Direction of the velocity fields in MDCK cells sheets migrating on 20- μm wide strip showing caterpillar like migration and abrogation of vortices. Each frame is 20 min apart and video is played at 7 frames per second. (Scale bar, 20 μm).

[Movie S5 \(MOV\)](#)



Movie S9. Deflection of pillars (2 μm diameter) in the narrow strips when cells migrate over them.

[Movie S9 \(MOV\)](#)



Movie S10. MDCK cells migrating on fibronectin strips of different widths in the presence of blebbistatin. Each frame is 4 min apart and video is played at 7 frames per second.

[Movie S10 \(MOV\)](#)